

# A Novel Image Segmentation Approach for Brain Tumor Detection Using Dual Clustering Approach

Dr.E.Mohan<sup>1</sup>, A.Annamalai Giri<sup>2</sup>, S.V.Aswin Kumer<sup>3</sup>

<sup>1</sup>Principal, P.T.LEE, Chengalvaraya Naicker College of Engineering and Technology, Kanchipuram, Tamilnadu, India.

<sup>2</sup>Professor, Department of Computer Science and Engineering, MLR Institute of Technology, Dundigal, Hyderabad, India.

<sup>3</sup>Assitant Professor, Department of Electronics and Communication Engineering, KL University, Green fields, Guntur, Andhra Pradesh, India.

## Abstract

Detection of brain tumors is a major issue nowadays due to the diagnosis of exact location and dimension of those tumors. This paper approaches image segmentation for brain tumor detection using dual clustering technique. Here the input image is separated by three channels of Hue, Saturation and Brightness and computing threshold for each channel to create a bitmap with the help of largest threshold computed from the three channels. Then the bitmap is segmented into black and white pixels to find out the nonoverlapping connected set of pixels and spots. The process of computing threshold includes the recognition of gray areas in the saturation and brightness channels.

**Index terms:** Dual Clustering Technique, Image segmentation, Medical Image Processing

## INTRODUCTION

Medicinal images have turned out to be basic in restorative analysis and treatment. These images assume a generous part in medicinal applications since specialists display enthusiasm for investigating the inward life systems[1]. Numerous

procedures have been created in light of X-beam and cross-sectional images like Computed Tomography (CT) or Magnetic Resonance Imaging (MRI), or other tomographic modalities (SPECT, PET, or ultrasound). Throughout the years, restorative image preparing has contributed a great deal in therapeutic applications; for instance, the utilization of image segmentation, image enlistment, and image guided surgery is so normal in medicinal surgery. The most established one is X-beam which has been connected by the specialists for over a century. In this strategy, electromagnetic radiation with the short wavelength and high vitality has been utilized. CT is another medicinal imaging strategy which utilizes X-beam in imaging inward body organs and structure. It delivers various parallel cuts of every organ by passing X-beam beats through the body. The other imaging method is Magnetic Resonance Imaging (MRI) as appeared in figure 1. It is a created therapeutic imaging strategy that works in light of attractive qualities and gives a lot of data about inside organs. This system has various advantages contrasted with different strategies because of which it is normally utilized as a part of therapeutic applications.

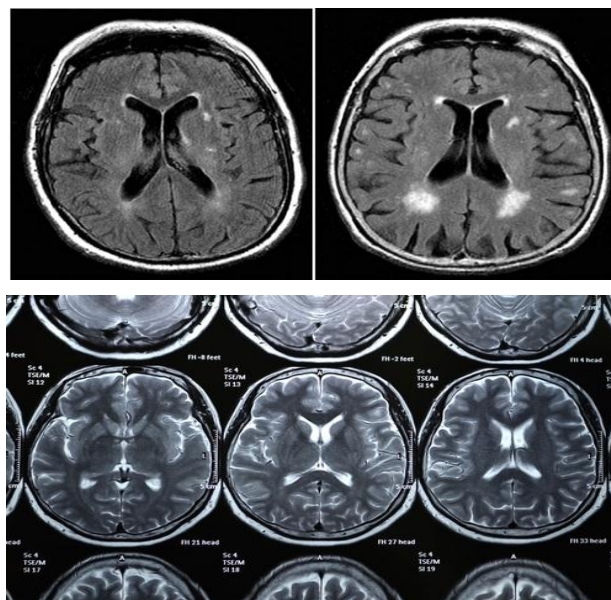


Figure 1 Magnetic Resonance Images

This system gives various parallel cuts for every organ in three measurements with the high difference between tissues. Notwithstanding, the information volume is excessively enormous for manual examination, which has been one of the greatest obstacles in MRI application. Working with MRI has a few disservices like commotion, power inhomogeneities, low differentiation between specific tissues, and halfway volume impacts in the division undertaking. The essential piece of restorative picture preparing is image segmentation. image segmentation is a technique for separating the Region of Interest (ROI) through a programmed or self-loader prepare. Many image segmentation strategies have been utilized as a part of medicinal applications to section tissues and body organs. A portion of the applications comprise of outskirts recognition in angiograms of coronary, surgical arranging, reproduction of surgeries, tumor identification and segmentation, a Mental health think about, useful mapping, platelets mechanized arrangement, mass location in mammograms, picture enlistment, heart segmentation and investigation of cardiovascular pictures, and so on. In restorative research, the division can be utilized as a part of isolating diverse tissues from each other, through removing and characterizing highlights. One of the endeavors is grouping picture pixels into anatomical locales which might be helpful in extricating bones, muscles, and veins. In this paper, the Dual clustering approach in Image Segmentation is proposed to detect the Brain tumor.

### PROPOSED METHODOLOGY

This paper Implements image segmentation for brain tumor detection using dual clustering technique. The Dual Clustering technique is a mix of three qualities of the picture: partition of the picture in light of histogram investigation is checked by high minimization of the groups (articles), and high inclinations of their outskirts. For that reason two spaces must be presented: one space is the one-dimensional histogram of brilliance  $H = H(B)$ , the second space – the double 3-dimensional space of the first picture itself  $B = B(x, y)$ . The primary space permits to gauge how conservative is dispersed the brilliance of the picture by computing negligible clustering  $k_{min}$ . Threshold brightness  $T$  relating to  $k_{min}$  characterizes the double (highly contrasting) picture – bitmap  $b = \varphi(x, y)$ , where  $\varphi(x, y) = 0$ , if  $B(x, y) < T$ , and  $\varphi(x, y) = 1$ , if  $B(x, y) \geq T$ [2]. The bitmap  $b$  is a question in double space. On that

bitmap, a measure must be characterized reflecting how minimized disseminated dark (or white) pixels are. Along these lines, the objective is to discover objects with great outskirts. For all  $T$  the measure  $P = G/(Q-L)$  must be figured (where  $Q$  is the contrast in shine between the protest and the foundation,  $L$  is the length of all fringes, and  $G$  is mean inclination on the outskirts). Greatest of  $P$  characterizes the segmentation[2].

The Dual Clustering approach begins with finding objects (spots on bitmap  $b$ ) and afterward assesses in double space the "quality" of their outskirts. At the end of the day, we are not searching for purposes of high slope, but rather for objects with great fringes. Coincidentally, this measure, which is exceptionally valuable for gray and color pictures, doesn't take a shot at Because each of the proposed measures has its own expert and contras. In this way, the calculation develop a mix PDC that reflects

- 1) Difference in brilliance between the question and the foundation measured by  $Q$ ,
- 2) Length of all fringes  $L$  reflecting the geometry of the question, and
- 3) Mean slope on the outskirts  $G$ , which reflects the nature of the fringe

$$P = \frac{G}{QL} \quad (1)$$

### PROPOSED ALGORITHM

The greater the  $P$  the better is the nature of segmentation. Picture Segmentation Principles already portrayed were actualized in a program, which executes the accompanying strides

1. Info picture is part in three channels: Hue, Saturation, and Brightness (Lightness).
2. Hazy areas on the picture are found (as regions with low saturation). These zones are rejected from the picture in the Hue channel.
3. For division the Dual Clustering (DC) system is connected to each channel ( $H, S, L$ ), i.e. for each channel  $P_{DC}(T)$  was computed as shown in figure 3 and the greatest  $P_{DC}$  and relating edge were kept ( $\{ P_{BDC}, T_B \}$ ,  $\{ P_{HDC}, T_H \}$ , and  $\{ P_{SDC}, T_S \}$ ).

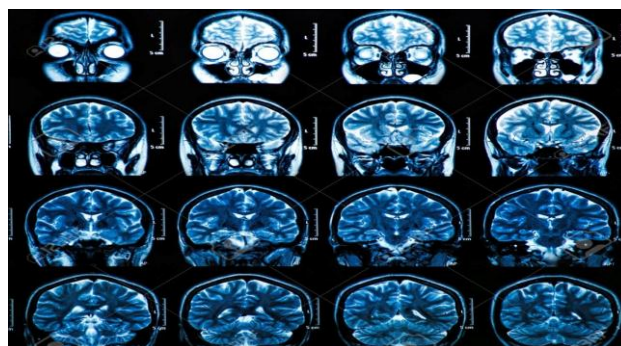
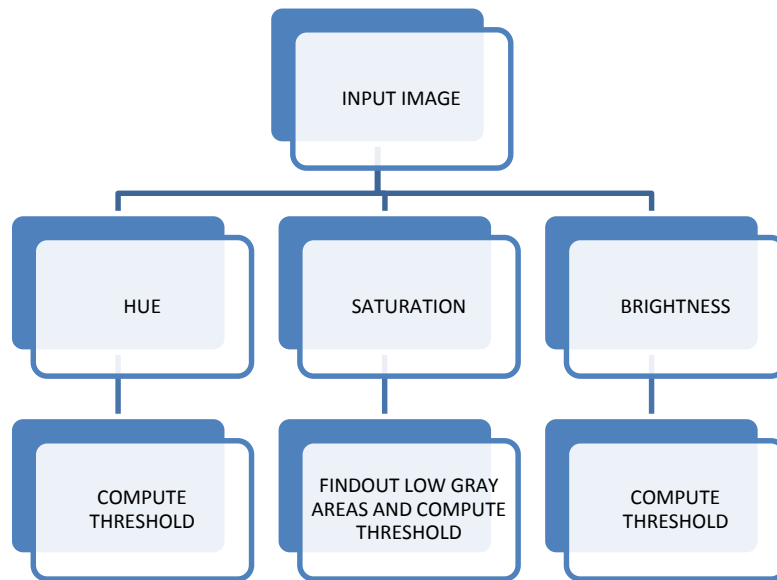


Figure 2. Lateral View of Magnetic Resonance Images

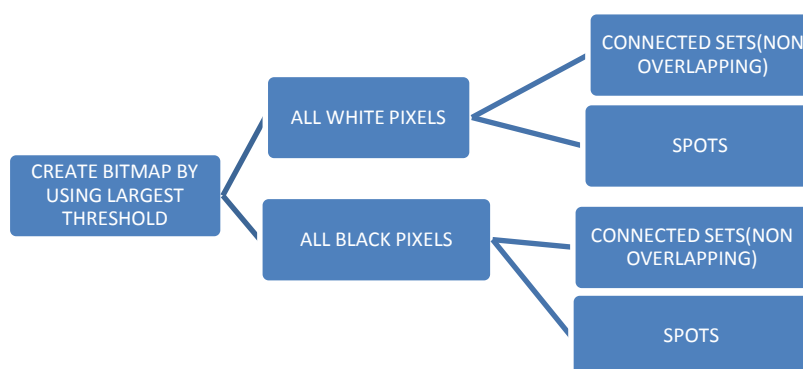


**Figure 3.** Block Diagram of Proposed Method (Stage I)

4. The biggest of three P DC esteems was picked and suitable T was utilized to make the bitmap speaking to a picked segmentation. That bitmap partitioned the total picture into two fragments: every single dark pixel and every white pixel. Each portion is then partitioned into non-covering associated sets of pixels –spots as shown in figure 4.
5. The calculation proceeds by applying recursively the Dual Clustering technique to each spot of the picture acquired at the past stride.
6. At each progression, spots are disposed of if
  - a) the spot is too little, or
  - b) the measure of grouping P DC for that spot sunk underneath some edge.

Segmentation stops when all spots are eliminated. The most tedious piece of Dual Clustering is finding greatest figuring P DC for every methodology (L, H, and S). For that reason, 255 high contrast bitmaps must be produced (for each of 255 estimations of given methodology). On each guide outskirts of all spots must be identified. Every pixel of a picture has 4 neighbors. The brilliance of that pixel and of every one of its

neighbors is known. Having these qualities one can find at which limits T that pixel will be a fringe pixel. As indicated by the definition, a pixel is an outskirts pixel if no less than one of its neighbors has a place with the spot and no less than one of its neighbors has a place with the foundation. Give B0 a chance to be the shine of the given pixel. Let  $B_j$  ( $j = 1, 2, 3, 4$ ) be the splendor of its neighbors. Give Bmin a chance to be the base of  $B_j$ . To start with, it must be noticed that a pixel with splendor B0 can be an outskirts purpose of some spot on a bitmap just if the edge T, that made that bitmap is under B0. Presently, if the bitmap was made by the limit T, which is littler than Bmin ( $T < Bmin$ ), at that point the focal pixel and every single neighboring pixel will have a place with the spot, and the focal pixel is not a fringe point. In the event that the limit is amongst Bmin and B0 the main issue will have a place with the spot and no less than one pixel (with brilliance =Bmin) will have a place with the foundation, i.e. the focal pixel will be an outskirts point. That data must be defined once for every pixel and after that, it winds up plainly known on which bitmaps (i.e. for which limits) it will be a fringe point.



**Figure 4** Block Diagram of Proposed Method (Stage II)

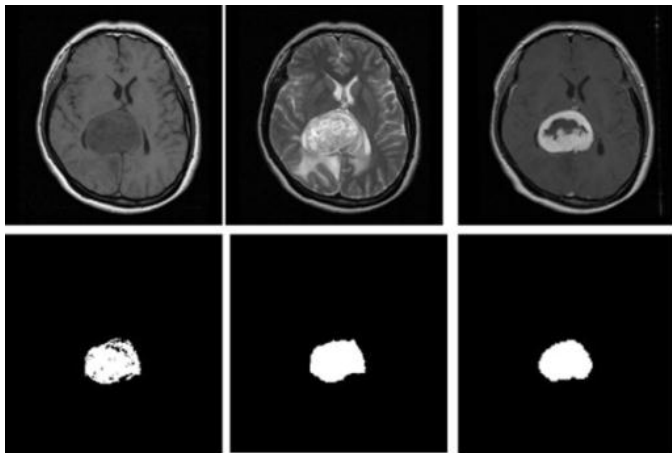
## SEGMENTATION ACCURACY

Segmentation Accuracy (SA) is defined as the ratio between the total number of classified pixels into the total number of pixels.

$$SA = \frac{\text{TOTAL NUMBER OF CLASSIFIED PIXELS}}{\text{TOTAL NUMBER OF PIXELS}}$$

## RESULTS AND DISCUSSION

In this area, the proposed calculation distinguishes the cerebrum tumor, appeared in figure 5. We portray some test results to look at the division execution of FCM, KFCM, Spatial Constraints KFCM (SKFCM), KFCM-F, GKFCM calculations with some numerical informational indexes and a few manufactured pictures. It is clear from the proposed calculation that it is performed well than FCM, KFCM, SKFCM, KFCM-F, GKFCM calculations. In Table-I, the proposed calculation delivered better PSNR and high division exactness than FCM, KFCM, SKFCM, KFCM-F, GKFCM calculations. Mean Square Error (MSE), Peak Signal to Noise Ratio (PSNR), Segmentation Accuracy (SA) strategies to know the productivity of the segmentation techniques.



**Figure 5** Outputs of the Proposed Algorithm and Morphological Filtering

**Table I:** Comparisons of Different methods of segmentation algorithms

Methods	MSE	PSNR	Segmentation Accuracy (%)
FCM	4.912	34.22	44.25
KFCM	1.235	42.56	50.55
SKFCM	0.910	49.68	66.75
KFCM-F	0.520	52.33	88.88
GKFCM	0.152	57.14	95.65
DUAL CLUSTERING	0.08	60.05	99.52

## CONCLUSION

In this paper, a Dual clustering algorithm is proposed for automatic segmentation of MR images to detect the brain tumor. This algorithm integrates the advantages of all existing algorithms and overcomes the demerits of the existing methodologies. In Experimental outcomes, the proposed technique is distinguished the brain tumor at culminate area, exact size and shape and it can be identified in a quickening plan.

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